# Measurement of Ultrasound Attenuation for Normal and Pathological Mice Breast Tissue using 10MHz Ultrasound wave.

#### \*MAHEZA IRNA MOHAMAD SALIM, MOHAMMAD AZIZI TUMIRAN, \*\*SITI NOR ZAWANI AHMMAD, \*\*ISMAIL ARIFFIN, \*\*ABDUL HAMID AHMAD, \*\*\*BUSTANUR ROSIDI, \*EKO SUPRIYANTO.

\*Dept. of Clinical Science and Engineering, Faculty of Biomedical and Health Science Engineering, \*\*Dept. of Electronics, Faculty of Electrical Engineering,

\*\*\*Chemical Engineering Pilot Plant,

Universiti Teknologi Malaysia.

Johor Bahru, 81310,

#### MALAYSIA.

<u>maheza@utm.my</u>, <u>iziza\_366@yahoo.com</u>, <u>snzawani2@siswa.utm.my</u>, <u>ismail@fke.utm.my</u>, <u>abdhamid@fke.utm.my</u>, <u>bustanur@fke.utm.my</u>, <u>eko@utm.my</u>

*Abstract:* - A new hybrid method that is based on the interaction of ultrasound and magnetic field has been developed for breast tumor detection. This method is capable to assess the acoustic and electric properties of normal and pathological breast tissue for characterization. In this study, the acoustic attenuation of normal and pathological mice breast tissue has been investigated from the ultrasound signal that is captured and recorded by the hybrid magnetoacoustic system. A total of 8 normal and 10 pathological mice breast tissue samples were studied by using a 10MHz ultrasound wave in transmission mode. The result of the attenuation measurement shows that pathological tissues attenuate more ultrasound compared to normal tissue. These results also agrees very well with previous research finding that indicates attenuation is lower for tissue with high proportion of cells such as mammary gland and fatty tissue and increases with collagen fibre content since the pathological tissue that were used in this study is multifocal, highly fibrotic and involve the entire mammary fat pad.

Key-Words: - Hybrid magnetoacoustic, 1D ultrasound, attenuation, normal and pathological, breast tissue.

# 1 Introduction

#### 1.1 Hybrid Magnetoacoustic Method.

Hybrid magnetoacoustic is a new breast cancer detection method that manipulates the interaction between acoustic and magnetic energy on random ionic particles inside a tissue. Biological tissue is a conductive element due to the presence of random charges that is mainly contributed by intra and extracellular diffusion that supports cell metabolism [1-6]. Propagation of ultrasound wave will cause charges inside the breast tissue to move at high velocity due to the back and forth motion of the wave [6-8]. Moving charges in the present of magnetic field will experience Lorentz Force. This force separates the positive and negative charges, producing an externally detectable voltage that can be collected using a couple of skin electrode [1-3].

This interaction has been manipulated to map conductivity data of biological tissue especially in impedance imaging. However, previous researches [1-8] apply magnetoacoustic method for conductivity mapping purposes only. The ultrasound wave that is used to stimulate ionic particle motion is not taken into account though its output delivers valuable information with regards to tissue mechanical properties [9]. Acoustic property such as attenuation has been proof so far to be very valuable in characterizing different biological tissues [10-14,17] and materials [18]. Hence, this paper presents ultrasound attenuation measurement from normal and pathological mice breast tissue for characterization purposes recorded by the system.

#### **1.2** Ultrasound attenuation

The attenuation of ultrasound wave that passed through tissues is unique and frequency dependant [10]. Previous study shows that ultrasound attenuation has a very high potential in characterizing biological tissue [17]. In the field of breast cancer study, specific normal and abnormal breast tissues such as fatty tissue, medullary carcinoma, infiltrative lobular carcinoma, fibrocystic and fibro fatty tissue have been characterized in [10,17] using ultrasound wave ranging below 10MHz by considering its attenuation coefficient. The same study were also done [15,16] to discriminate benign and malignant breast tissue by accessing the tumor backscatter echo, speed of sound and attenuation coefficient. However, the type of benign and malignant tissue used in these studies is not stated specifically. In [16], discrimination has been done by comparing their frequency dependant attenuation and speed of sound of ultrasound wave ranging from 2 to 9MHz.

# 2 Materials and Method

## 2.1 Mice Strain

The used of animal in this study is approved by the National University of Malaysia Animal Ethics Committee. 2 sets of mice strain FVB/N-Tg MMTV PyVT 634 Mul and its control strain FVB/N is obtained from the Jackson Laboratory, USA.

For the transgenic mice set, hemizygote male mice were crossed to female noncarrier to produce 50% offspring carrying the PyVT transgene. The Mice offsprings were palpated every 3 days starting from 12 weeks of age to identify tumors in which earliest tumor development starts at 5 weeks of age. Adenocarcinoma that arises in virgin and breeder females were observed to be multifocal, highly fibrotic and involve the entire mammary fat pad [19]. Mice carrying the PyVT transgene also show loss of lactational ability since the first pregnancy [19].

In this study, 8 normal and 10 pathological breast tissue specimens were harvested from 4 normal and 5 transgenic virgin, female mice at the age of 18 weeks.

### 2.2 Mice Anesthesia and Surgery

Individual mouse was restrained by using a plastic restrainer before anesthesia. Anesthesia was performed by using the Ketamin-Xylazil-Zoletil cocktail dilution. 0.2ml of the anesthetic drug was administered intravenously from the mouse tail and an additional of 2ml of anesthetic drug was delivered intraperitoneally for about 2 hours sleeping time. Fur around the breast area was shaved. Normal and pathological mammary tissue were harvested from the mice while they were sleeping. Mice were then killed by using drug overdose method. Before the specimens were cut into the required shape and thickness, their physical appearance was first observed.

### 2.3 Ultrasonic Analysis

Excised breast specimens were cut down to an approximately 1cm x 1cm square shape with thickness of 1mm immediately after the surgery [10]. Part of the specimens was immersed in buffered formalin for

Histological examination. The specimens were immersed in gel that is located between the ultrasound transmitter and receiver. Ultrasound analysis was started and performed at a constant temperature of 21°C by using the insertion loss method described elsewhere previously [10-14]. In the Insertion loss method, attenuation of ultrasound travelling through the tissue immersed in the gel was deducted by the attenuation of ultrasound propagated through the gel when tissue was removed.

The hybrid magnetoacoustic system recorded the ultrasound signal in time domain. Signal is captured by using a frequency sampling of 2.5GHz. All signals were first filtered by using the  $2^{nd}$  order Low Pass Chebyshev filter to remove the unwanted signal over 50 MHz. The signals were then converted to frequency domain for analysis. Squared spectrum of the signal was calculated in Matlab. Attenuation coefficient in dB is calculated as [18, 20]:

Attenuation:  $20 \log_{10}[I_t/I_g](1)$ 

Where  $log_{10}I_t$  is the squared spectrum of the ultrasound signal propagating through gel with tissue and  $log_{10}I_g$  is the square spectrum of the ultrasound signal propagating in gel without tissue.

# **3** Result and Discussion

### 3.1 Tissue Appearance



Fig 1: Physical appearance of a pathological breast masses from an individual mouse subject.



Fig 2: Physical appearance of a normal breast masses from four individual mouse subjects.

#### 3.2 Ultrasound Analysis result.



Fig. 3: Original ultrasound signal recorded by the system and its corresponding filtered signal



Fig. 4: FFT of the ultrasound signal calculated in Matlab



Fig. 5: Mean Squared Spectrum of the filtered ultrasound signal



Fig. 6: Mean and standard deviation of ultrasound attenuation for normal and pathological mice breast tissue at 10MHz.

Figure 3, 4 and 5 shows the signal processing steps to determine the attenuation value of the breast tissue specimens. Final attenuation value was calculated by substituting the peak mean squared spectrum of the signals into equation (1). The result in Fig. 6 shows the mean attenuation for these tissues permilimeter at 10MHz. The mean result shows that pathological tissue attenuates more ultrasound compared to normal tissue at the same propagation distance. These results also agrees very well with previous research finding [17] that indicates attenuation is lower for tissue with high proportion of cells such as mammary gland and fatty tissue and increases with collagen fiber content since the pathological tissue that were used in this study is multifocal, highly fibrotic and involve the entire mammary fat pad [19].

However, this result contradicts with our previous simulation result on the attenuation of normal and

pathological breast. The simulation was calculated based on attenuation coefficient in [20], in which the attenuation of normal tissue is higher than the pathological tissue.

# 4 Conclusion

A new hybrid method that capable to measure acoustic and electric properties of tissues has been developed for breast cancer detection. The present paper reports on the measurement of acoustic property of tissue namely acoustic attenuation. 8 normal and 10 pathological mice breast tissues specimens have been studied by using the insertion loss method. Result shows that pathological tissues attenuate more ultrasound compared to normal tissue as attenuation is low in tissue with high proportion of cells and increasing with collagen content.

### References:

[1] Han Wen, Jatin Shah and Robert S. Balaban, Hall Effect Imaging, *IEEE Transactions On Biomedical Engineering*, Vol 45, No 1, 119-124, January 1998
[2] Han Wen, Eric Bennett, Jatin Shah, Robert S. Balaban, An Imaging Method using Ultrasound and Magnetic Field, *IEEE Ultrasonic Symposium*, 1997.

[3]Han Wen, Eric Bennet, The Feasibility of Hall Effect Imaging In Humans, 2000 IEEE Ultrasonic Symposium, pg 1619-1622

[4] Amalric Montalibet, Jacques Jossinet, Adrien Matias, Dominique Cathignol, Interaction Ultrasound –Magnetic field: Experimental set up and Detection of the interaction current, 2000 IEEE Ultrasonic Symposium, pg 533-536

[5] Y. Su, S. Haider, A. Hrbek, Magnetoacousto Electrical Tomography: A new Imaging Modality for Electrical Impedance, 2007 IFMBE Proceeding 17, pp 292-295, 2007

[6] M. I. M. Salim, M. A. Tumiran, S. N. Makhtar, B. Rosidi, I. Ariffin, A. H. Ahmad, E. Supriyanto, Hybrid Magnetoacoustic Method for Breast Tumor Detection: An In vivo and In vitro Modelling and Analysis. WSEAS Transactions on Information Science and Application, September 2010.

[7] Boris Cigale, Smilijan Sinjur, Damjan Zazula, Automated Quantitative Assessment of perifollicular Vascularization Using Power Doppler Ultrasound Images. *WSEAS Transactions On Computers*, Vol 9, 2010. [8] Elene B. Martin, Jose M. Vega, Effect of a thin floating fluid layer in parametrically Forced waves. *WSEAS Transactions on Fluids Mechanics*, Vol 3, 2008.

[9] M. I. M. Salim, M. A. Tumiran, S. N. Makhtar, B. Rosidi, I. Ariffin, A. H. Ahmad, E. Supriyanto, Quantitative analysis of Hybrid Magnetoacoustic Method for Detection of normal and pathological Breast Tissue. *Proceeding of 12<sup>th</sup> WSEAS International Conference on Automatic Control, Modelling and Simulation*, pg 144-149, 2010.

[10] L. Landini and R. Sarnelli, Evaluation of the attenuation coefficient in normal and pathological breast tissue. *Medical and Biological Engineering and Computing*, IFMBE, 1986.

[11] S. G. Ye, K. A. Harasiewicz, C. J. Pavlin, and F. S. Foster, Ultrasound Characterization of Normal Ocular Tissue in the Frequency Range from 50 MHz to 100 MHz. *IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control*, Vol. 42, No. 1, January 1995

[12] Takahiro Iwamoto, Yoshifumi Saijo, Naohiro Hozumi, Kazuto Kobayashi, Nagaya Okada, Akira Tanaka, and Makoto Yoshizawa, High Frequency Ultrasound Characterization of Artificial Skin. *30th Annual International IEEE EMBS Conference*, Vancouver, British Columbia, Canada, August 20-24, 2008

[13] M. Lebertre, F. Ossant, L. Vaillant, S. Diridollou, F. Patat, Human Dermis Ultrasound Characterization: Backscattering Parameters Between 22-45 MHz. 2000 IEEE Ultrasonic Symposium.

[14] Balasunder I. Raju and Mandayam A. Srinivasan.Characterization of human fingertip and forearm skin using attenuation coefficient of high frequency ultrasound. *IEEE Ultrasonic Symposium*, 2000.

[15] B. Alacam, B. Yazici, N. Bilgutay. Breast tissue characterization based on ultrasound RF Echo Modeling and tissue morphology. *Proceeding of 25<sup>th</sup> Annual International Conference of the IEEE EMBS*, 2003.

[16] P.D. Edmonds, C. L. Mortensen, Ultrasonic tissue characterization for breast biopsy specimen. *IEEE Symposium*, 1987.

[17] Andrzej J. Surowiec, Stanislaw S. Stuchly, J. Robin Barr and Arvind Swarup, Dielectric properties of Breast Carcinoma and Surrounding Tissue. *IEEE Transaction on Biomedical Engineering*, Vol 35, No 4, pg 257-263. [18] A.Q. Chen, S. Freear, D. M. J. Cowell, Measurement of solid in liquid content Using Ultrasound Attenuation. 5<sup>th</sup> World Congress on Industrial Process Tomography, Bergen Norway.

[19] JAX Mice Database: MMTV-PyVT strain, The Jackson Laboratory, USA. 5<sup>th</sup> September 2010. http://jaxmice.jax.org/strain/002374.html.

[20] Thomas L. Szabo, *Diagnostic Ultrasound Imaging Inside Out*, Elsevier Academic Press, 2004.